

Theory:

## Radial sampling interactions in multi-dimensional sparse encoding problems using a joint decoding-reconstruction framework

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Introduction + Theory Methods Results Discussion Background: a) h) All reconstructions were assessed using correlation Joint decoding and Vessel Simulated encoding-trajectory interactions: Many MR measures are indirectly inferred selective (R<sup>2</sup>) with ground truth data Joint reconstruction reconstruction gives 1. Same trajectory for each encoding + 4x4 from multiple measurements. (e.g. the tag selective tagging and alternating trajectory performed best (Figs 3 more degrees of Hadamard encoding of 3 vessels and tagging and the control image in arterial spin labelling and 4) freedom and produces static tissue (Fig 1a – no rotation) or multi-TE images for relaxometry). The multidimensional point spread function (mbetter results 2. Different trajectory for each encoding Reconstruction and decoding of the signal of PSF) observations (Fig 5): Especially when (45° rotated) + 4x4 Hadamard encoding interest are often treated separately. The m-PSF is symmetrical (Signal from optimised for energy (Fig 1a) Instead, treating them jointly opens up new component A aliases into component B in the distribution of data 3. Different trajectory for every other degrees of freedom. same way that signal from B aliases into A, etc.) The m-PSF can be used encoding with half the number of Modern MRI is often undersampled and · Component mixing determined by energy of as a tool to study spokes per encoding compared with reconstructed with compressed sensing. off-diagonal blocks interactions between method 1 and 2 + paired 8x4 Hadamard Alternating trajectory nulls high energy trajectory and other encoding (Fig 1b) • The acquisition operator. E. and the pointcomponent (background) types of signal encoding Reconstruction strategies: spread-function (PSF = E'E) determines the · Diagonal blocks unaffected by which spokes Simple case and theory Reconstruct first – then decode (Fig 2a) spreading of artefacts and is generally shift are acquired in which encoding presented here. In-vivo Decode first - then reconstruct (Fig 2b) invariant. trials presented in Joint reconstruction + decoding (Fig 2c) Fig 1 - Four components (3 vessels + 1 background) are Incoherence of *E* is essential for compressed Reconstruction approach abstract #1073 encoded into four (a) or eight (b) encoded images that are sensing<sup>1</sup> to work. acquired with a radial trajectory that is rotated for some of the Decode + recon Recon + decode Joint Applications beyond ASL Compressed sensing optimisation using When reconstruction and decoding of the encodings include e.g. 4D phase the Fast Iterative Soft Thresholding signal are treated separately, we can only imaging<sup>4</sup>. Algorithm (FISTA<sup>3</sup>) was used minimising influence the incoherence of **E** through choice sparsity of the image in its native space: of trajectory. When considering reconstruction and  $cost = \frac{1}{2} |Ex - d|_2^2 + \lambda |x|_1$ recor + decoding jointly, a more optimal combination λ = 5 for all methods of trajectory and encoding can be developed. Data + simulation setup: In this work: 10 augmentations of a digital VE-ASL Watch a pre-recorded We used an example framework to investigate phantom were used and 10 instances of presentation here sampling and encoding interactions: golden complex gaussian noise were added to Fig 2 – To find a property of interest you can either reconstruct angle radially sampled vessel-encoded arterial then decode (a), decode and then reconstruct (if same sampling lternatir each before reconstruction. spin labelling (VE-ASL)<sup>2</sup>. points) (b), or do a joint reconstruction and decoding. N/A The background component had We developed a tool called the approximately 10 times higher signal nstruction quality - 16 spokes - realistic backgro multidimensional point-spread-function (m-Meet the author: than the vessel components. Total Tue 11<sup>th</sup> August 2020, 10-PSF) to explore these types of interactions. Fig 3 - Sharp and detailed reconstructions with only 16 spokes can be background suppression was also tested 12 AM (UTC) acquired with joint reconstruction and using the alternating spokes The m-PSF was generated by transforming (component 4 set to zeros). approach (E'E) a delta function centred in each Images were reconstructed from a total component and measuring its effect on every of 16 or 64 spokes spread across the Fig 5 – Using same spokes each encoding other component. results in no mixing of components (a). If each encodings. different traiectory all components mix (b). With the alternating REFERENCES:

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Fig 4 - Varying spokes each encoding is bad because the static tissue swamps the vessel components. The alternating spokes approach removes the background but samples more locations in k-space than using the same spokes each encoding.



annroach one can ston one component from mixing (c). Through matching sampling and encoding we control aliasing in the component direction.

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